

# Simulation and Optimization of Biomedical Devices.

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# SimLab: Highly Scalable Fluids and Solids Engineering

#### ► Goals:

- Large scale CFD on massively parallel computers
- Finding ways towards peta- and exascale computing
- Porting and scaling of CFD applications and tools
- Design of parallel PDE solvers (FEM and FVM)
- Supporting researchers on HPC and CFD

#### ► Know-How:

- Finite Element Methods, Galerkin/Least-Squares (GLS), Discontinous Galerkin (DG) and Finite Volume Methods
- Cartesian Grid-based methods and unstructured grid methods
- Mesh partitioning and mapping
- Automated parallel/distributed mesh generation
- Shape optimization for fluids
- Haemodynamics
- etc.

#### Applications:

- Massively-parallel simulations,
- Shape Optimization Framework,
- Single-surface geometry representation.

# SimLab: Highly Scalable Fluids and Solids Engineering

#### ► Current HPC Projects:

- Large Scale Mesh Decomposition
- Tree-Code-Based Finite Volumes
- Peta-Scaling of XNS (RWTH, Behr)
- Peta-Scaling of ZFS (RWTH, Schröder)
- Current Support Projects
  - COPA-GT (CERFACS)
  - DIGITAL-X (DLR)
  - openFOAM on BGQ (Siemens)

#### Current CFD Projects

- Spatially Resolved Simulation of Packed Bed Chromatography (FZJ, Lieres)
- Large-eddy simulations in support of accurate blood flow and blood damage simulations (RWTH, Behr)
- Discontinuous Galerkin method for coupled aeroacoustics (RWTH, Schröder)



## **XNS** Overview



- ▶ The set of governing equations:
  - Advection-Diffusion
  - Incompressible Navier-Stokes
  - Compressible Navier-Stokes
  - Shallow-Water Equations
- Highlights of XNS
  - Portable and parallel FE-code
  - Mesh update techniques
  - Viscoelastic fluids
  - Large-Eddy Simulations
  - Free surface flows
  - Discretization: (fully implicit) space-time or semi-discrete
  - Shape Optimization



## Simulation performance Blue/Gene 2006



Expected scaling up to 2048 to 4098 PEs.

#### Parallel Linear Solver

▶ PDE solver heavily depends on solutions of linear equation systems:



- GMRES solver, (block-)diagonal and ILU preconditioning,
- Utilizing a distributed vector-matrix multiplication.



## Distributed Vector-Matrix Multiplications



#### Scalasca



## Simulation performance JUGENE 2008



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## Validation DeBakey Blood Pump

- Experimental results provided by MicroMed,
- CFD validation done with XNS flow solver:



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## FDA's 'Critical Path' Initiative

- ▶ Round-Robin Study with 28 participating research groups.
- Simple Geometry:



Centerline velocity at Re = 500 from [Stewart 2012] :



#### FDA's 'Critical Path' Initiative

Centerline velocity at Re = 500 with XNS:



Tetrahedral mesh with 13 million elements

# FDA's 'Critical Path' Initiative

Scalability on JuQueen:



- ▶ BG/Q has four floating point units per core,
- XNS is able to exploit them efficiently.

# Spatially Resolved Chromatography Simulations

Important unit operation for compounds separation:



(a) Industrial scale

(b) Laboratory scale

- Collaboration project with Eric von Lieres (FZJ, IGB-1 Biotechnology),
- Common homogeneity assumptions not appropriate at small scales,
- Status Feb. 2012 : 750 beads simulation (flow only),
- ▶ Status Feb. 2013 : 8000 beads simulation (flow + mass-transfer).
- ▶ New model for scale-up (laboratory scale to industrial scale) needed.

# Spatially Resolved Chromatography Simulations

• Example simulation with 1257 randomly packed beads:



- Simulation contradicts homogeneity assumption.
- Current challenges are mesh generation and visualization.

# Shape Optimization in an Engineering Context

Shape optimization projects at CATS:



(a) blood pump design

(b) extrusion die design

- Interface with CAD programs needed in two projects:
  - MicroMed Inc: Robust shape optimization for artifical blood pumps.
  - ► Excellence Cluster EXC 128: A2 Individualized production.
- Strong geometric constraints:
  - production limits,
  - design limits.
- Fundamental needs:
  - watertight model,
  - arbitrary topology possible,
  - NURBS compatible,
  - easy to parameterize.



# **T-Splines**

Typical geometry in a CAD system:



▶ NURBS [Versprille 1975]:





► T-spline [Sederberg 2003]:



# Model Generation: T-Splines

T-spline spaces:



(a) index/parameter space



T-spline surface is calculated by:

$$\mathbf{C}(oldsymbol{ au}) = rac{\sum\limits_{i}eta_i \mathbf{P}_i B_i(oldsymbol{ au})}{\sum\limits_{i}eta_i B_i(oldsymbol{ au})}.$$

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# Model Generation: Toolchain

- Basic mesh generation:
  - ▶ Rhino<sup>TM</sup> for CAD model cleanup,
  - ▶ Pointwise<sup>TM</sup> for FE mesh generation,
  - file I/O with IGES.
- Shape parameterization with:
  - ▶ in-house Matlab<sup>TM</sup> toolbox (since 2007),
  - B-splines, T-splines (merge, glue and fit),
  - in-house graphical editor for the shape parameterization,
  - file I/O with IGES, STL and XML.
- ► Geometry kernel:
  - in-house Fortran 90 library (shade),
  - $\gamma(\alpha), \frac{d\gamma(\alpha)}{d\alpha},$
  - file I/O via XML.







## Shape Optimization Problem

- Problem: How to place a bypass?
- Minimize blood damage with

$$J(\mathbf{v}, \boldsymbol{\alpha}) = 2 \int_{\Omega_{\rm obs}(\boldsymbol{\alpha})} \boldsymbol{\varepsilon}(\mathbf{u}) : \boldsymbol{\varepsilon}(\mathbf{u}) d\mathbf{x}$$

as a simple hemolysis model.

Navier-Stokes equations viewed by a fluid dynamicist:

$$\rho\left(\frac{\partial \mathbf{u}}{\partial t} + \mathbf{u} \cdot \boldsymbol{\nabla} \mathbf{u} - \mathbf{f}\right) - \boldsymbol{\nabla} \cdot \boldsymbol{\sigma}(\mathbf{u}, p) = \mathbf{0}, \qquad \boldsymbol{\nabla} \cdot \mathbf{u} = 0 \qquad \text{on } \Omega.$$

Navier-Stokes equations viewed as a generic state equation:

$$\mathbf{c}(\mathbf{u},p;\mathbf{x})=\mathbf{0}.$$

▶ Optimal shape design problem evaluates  $\alpha \in \mathcal{A}_{ad} \subset \mathbb{R}^n$ :

$$\begin{array}{ll} \mbox{minimize} & J(\mathbf{u},p,\boldsymbol{\alpha}), \\ \mbox{subject to} & \mathbf{c}(\mathbf{u},p;\mathbf{x}(\boldsymbol{\alpha})) \mbox{ on } \Omega(\boldsymbol{\alpha}), \\ & \boldsymbol{\alpha} \in \mathcal{A}_{ad}. \end{array}$$



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# Shape Optimization Problem (cntd)

Reformulated problem:

$$\begin{array}{ll} \mbox{minimize} & J(\mathbf{x},\mathbf{v},\boldsymbol{\alpha}), \\ \mbox{subject to} & \mathbf{0} = \mathbf{c}(\mathbf{v};\mathbf{x}(\boldsymbol{\alpha})) \\ & \mathbf{0} = \mathbf{d}(\mathbf{x}(\boldsymbol{\alpha});\boldsymbol{\gamma}(\boldsymbol{\alpha})) \\ \mbox{on} & \Omega = \Omega(\boldsymbol{\alpha}) \mbox{ with } \boldsymbol{\alpha} \in \mathcal{A}_{ad} \end{array}$$

with

$$\mathbf{v} = \begin{pmatrix} \mathbf{u} \\ p \end{pmatrix}$$

for the incompressible Navier-Stokes states.

Two approaches to solve this problem:

- ► As one problem (SAND, fully-coupled),
- As a coupled problem (NAND, black-box approach).

Our way:

- Solution as a coupled problem simplifies the use of existing solver,
- Gradient-based approach.



## Artificial graft optimization Re 200

• The initial shape  $(J_{init} = 118)$ :



• Optimal shape  $(J_{opti} = 88.3)$  with 24 parameters using the  $C^0$ -merge:



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#### Discussion

- ► Finite Elements for Fluids:
  - General FEM for flow problems,
  - Multi-physics.
- Issues in Massively-parallel Simulations:
  - Profiling,
  - Mesh generation
  - Mesh partitioning and mapping,
  - Visualization.

#### Applications:

- Massively-parallel simulations,
- Shape Optimization Framework,
- Single-surface geometry representation.







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